

The glycolipid GM1 reshapes asymmetric biomembranes and giant vesicles by curvature generation

Raktim Dasgupta^{a,1}, Markus S. Miettinen^a, Nico Fricke^{a,2}, Reinhard Lipowsky^a, and Rumiana Dimova^{a,3}

^aDepartment of Theory and Bio-Systems, Max Planck Institute of Colloids and Interfaces, 14424 Potsdam, Germany

Edited by Steven G. Boxer, Stanford University, Stanford, CA, and approved April 25, 2018 (received for review December 24, 2017)

The ganglioside GM1 is present in neuronal membranes at elevated concentrations with an asymmetric spatial distribution. It is known to generate curvature and can be expected to strongly influence the neuron morphology. To elucidate these effects, we prepared giant vesicles with GM1 predominantly present in one leaflet of the membrane, mimicking the asymmetric GM1 distribution in neuronal membranes. Based on pulling inward and outward tubes, we developed a technique that allowed the direct measurement of the membrane spontaneous curvature. Using vesicle electroporation and fluorescence intensity analysis, we were able to quantify the GM1 asymmetry across the membrane and to subsequently estimate the local curvature generated by the molecule in the bilayer. Molecular-dynamics simulations confirm the experimentally determined dependence of the membrane spontaneous curvature as a function of GM1 asymmetry. GM1 plays a crucial role in connection with receptor proteins. Our results on curvature generation of GM1 point to an additional important role of this ganglioside, namely in shaping neuronal membranes.

lipid nanotubes | gangliosides | giant vesicle | spontaneous curvature | membrane

Gangliosides (1, 2), glycosphingolipids that contain sialic acid residues, are important components of all animal cell membranes and are more abundantly expressed in the nervous system. These complex lipids consist of a large saccharidic head group and a two-tail hydrophobic moiety (ceramide). The vast diversity in their structure stems from the heterogeneity in the oligosaccharide chain. Even though gangliosides were discovered already in 1939 (3), their role in the regulation of many biomembrane functions is not yet understood. It is now known that despite being present as the smallest fraction among the lipids of different cell plasma membranes, gangliosides modulate a number of cell surface receptor activities and play a crucial role in neuronal differentiation and development processes. Importantly, gangliosides accumulate at high levels in brain tissue and are believed to be related in major neurological disorders such as the Guillain-Barré syndrome, Alzheimer's disease, and parkinsonism (4, 5). The monosialoganglioside GM1, widely considered as the ganglioside paradigm displaying the characteristic features identifying gangliosides, has been shown to affect membrane curvature (1, 2) and can be expected to strongly influence the neuron morphology. The curvature effect of GM1 is not only expected to be important in specific tubular morphologies of neuron cells but also, as recently pointed out, in the formation of long connecting nanotubes between cancer cells (6) promoting direct intercellular transfer of cytoplasmic components, which may even include chemotherapy-resistive genes (7). However, so far, the effect of GM1 on membrane curvature is only poorly understood. Although the artificial model membrane systems like small unilamellar vesicles of very high curvature or thin membrane nanotubes pulled out of giant unilamellar vesicles (GUVs) are being often used to perform quantitative investigations on the curvature-related properties of membrane lipids (8, 9), there are some major challenges in characterizing gangliosides such as GM1 using these techniques. First, GM1 molecules have a prominent asymmetrical localization in the

outer cell membrane (10), and the asymmetric distribution is crucial for their effect on membrane curvature. However, mimicking such an asymmetry in model membrane systems such as GUVs poses a major challenge. Second, the above-mentioned techniques require associating the GM1 molecules with suitable fluorophores. A very widely employed method for staining GM1 in cell membranes is to use a fluorophore moiety conjugated with cholera toxin that subsequently binds to GM1 (11–15). However, the curvature generated by these aggregates is significantly different from that of individual GM1 molecules both in sign and value (6, 14). Alternative approaches of using labeled GM1, as for example the boron-dipyrromethene (BODIPY)-GM1 complex, suffer from the drawback that the labeling alters the molecule partitioning in domains (16) and increases the volume of the hydrophobic part of GM1, thereby changing its molecular shape from the natural inverted conical shape (17). Furthermore, in biological systems, compositional differences between various membrane compartments are well known and are believed to be primarily driven by sorting of lipids coupled to membrane curvatures (18-21). The enrichment of GM1 at the tips of the echinocyte spiculae and curved exovesicles, attributed to the intrinsic spontaneous curvature of the molecule, is well known (17). In addition, GM1 plays very important roles in axonal growth in neuron cells and has been shown to be highly enriched in the tubular morphology of axons (22). Although these observations

Significance

The multifaceted involvement of GM1 as a ligand in many cellular functions has been well recognized. We find that GM1 readily desorbs from the membrane of cell-sized model biomimetic systems (giant unilamellar vesicles). The desorption is unbalanced, creating an asymmetry between the bilayer leaflets. This results in reshaping weakly curved membranes into nanotubular invaginations stabilized by the membrane spontaneous curvature, which we quantify experimentally. Computer simulations confirm the experimental results. Uncovering the role of GM1 as a fine regulator of membrane curvature broadens our perspective on its important function in reshaping neuronal membranes and emphasizes that GM1 desorption can strongly affect the cell membrane morphology.

Author contributions: M.S.M., R.L., and R. Dimova designed research; R. Dasgupta, M.S.M., and N.F. performed research; R. Dasgupta, M.S.M., N.F., and R. Dimova analyzed data; and R. Dasgupta, R.L., and R. Dimova wrote the paper.

The authors declare no conflict of interest.

This article is a PNAS Direct Submission.

This open access article is distributed under Creative Commons Attribution-NonCommercial-NoDerivatives License 4.0 (CC BY-NC-ND).

¹Present address: Laser Biomedical Applications Section, Raja Ramanna Centre for Advanced Technology, 452013 Indore, India.

²Present address: Department of Molecular Physiology and Biophysics, Vanderbilt University, Nashville, TN 37232.

³To whom correspondence should be addressed. Email: dimova@mpikg.mpg.de.

This article contains supporting information online at www.pnas.org/lookup/suppl/doi:10.1073/pnas.1722320115/-/DCSupplemental.

Published online May 14, 2018.

provide qualitative evidence for the curvature effect of GM1, no quantitative estimates for the GM1-generated curvature have been obtained so far.

Here, we report the results of our investigations on GM1-doped membranes in which GM1 distributes asymmetrically between the two membrane leaflets of giant vesicles. This asymmetry generates spontaneous tubulation in GUVs, with tubes being stabilized by negative spontaneous curvature. We developed an assay to assess the asymmetric distribution of GM1 across the membrane. To measure the spontaneous curvature associated with this asymmetry, we used an experimental approach for which a membrane nanotube could be pulled from a giant vesicle using an optically trapped latex bead as a handle. In addition, the force transducer property of the optical trap allowed for measuring tube pulling forces with high precision (23, 24). We demonstrate that via pulling inward and outward tubes on the same vesicle, it is possible to assess mechanical properties such as the membrane bending rigidity and spontaneous curvature without considering the membrane tension. The results for the spontaneous curvature are compared with coarse-grained molecular-dynamics simulations.

Results and Discussion

Inward Tubulation Resulting from Asymmetric GM1 Desorption. GUVs were prepared from palmitoyloleoylphosphatidylcholine (POPC) and various mole fractions of GM1 in 1 mM Hepes buffer (Materials and Methods and SI Appendix, section S1). Note that, at room temperature, membranes containing GM1 above around 5 mol% exhibit gel-like domains (25). Thus, observations on vesicles with higher content of GM1 were performed at 40 °C; for a partial phase diagram of the system, see ref. 25. After preparation, the vesicles appeared clean, without internal structures. Upon 10-fold (isotonic) dilution in vesicle-free 1 mM Hepes solution, the GUVs exhibited a large number of internal tubes (Fig. 1 and SI Appendix, section S2) (similar observations were made in aqueous solutions without Hepes). This observation is consistent with protrusions detected on asymmetric supported bilayers (26). The tubes we observe can adopt cylindrical or necklace-like morphologies depending on their length and growth kinetics (27).

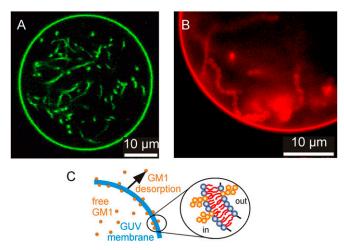


Fig. 1. Vesicles prepared from POPC with 10 mol% GM1 in 1 mM Hepes exhibit internal tubes upon 10-fold dilution; observed at 40 °C. (A) Confocal cross-section of a GUV labeled with 0.1 mol% BODIPY-GM1. (B) Epifluor-escence image of a part of a GUV labeled with 0.1 mol% TR-DHPE. The necklace-like structure of the membrane tubes is visible. (C) Schematic illustration of the asymmetric distribution of GM1 across the membrane resulting from GM1 desorption upon dilution of the GUV external medium. The *Inset* illustrates the decreased density of GM1 on the outer leaflet and the associated generation of negative spontaneous curvature in the membrane, which stabilizes inward tubes.

The formation of internal nanotubes in the GM1-doped vesicles upon dilution of the external medium suggests that an asymmetric distribution of GM1 between the leaflets arises by the desorption of GM1 from the outer leaflet (Fig. 1C). As a consequence, the density of GM1 in the inner leaflet exceeds the density in the outer leaflet, which gives rise to a negative spontaneous curvature. To confirm this conclusion, we carried out experiments in which GM1 was externally added to the tubulated vesicles (SI Appendix, section S3). For small amounts of added GM1, the in-tubes were retracted, suggesting a symmetric distribution of the ganglioside resulting in zero spontaneous curvature. Upon further addition of GM1, the formation of external tubes was observed, indicating the generation of positive spontaneous curvature as more GM1 was inserted into the outer leaflet of the vesicle membrane.

Assessing the Concentration of GM1 in Each Leaflet. To assess the amount of GM1 in the individual leaflets of 10-fold diluted vesicles with internal tubes, we developed the following experimental assay based on electroporation (*SI Appendix*, section S4). First, Alexa Fluor-conjugated cholera toxin B (CTB-Alexa) was added to the vesicle solution. Since the vesicles were intact, each CTB predominantly binds to five GM1 molecules present over the outer leaflet of the vesicle membrane. The fluorescence signal appeared uniform, suggesting no microscopic phase separation as observed in other membrane compositions (12). The vesicles were imaged after 10-min incubation time under a confocal microscope. After recording the fluorescence from CTB-Alexa bound to the GM1 molecules only in the outer leaflet (Fig. 2A), a short electric DC pulse (50-ms duration, amplitude between 7 and 10 kV/m) was applied. The electric field induces the formation of micrometer-sized pores in the membrane (28-31). Consistent with the negative spontaneous curvature, the membrane in the vicinity of the pore was observed to curl outward (SI Appendix, Fig. S4). The large pores allowed exposing the inner membrane leaflet to the external solution containing CTB-Alexa and maybe also interleaflet exchange along the pore rim. This led to a visible increase in the membrane fluorescence resulting from additional binding of CTB to GM1 in the inner leaflet (Fig. 2 B and C). The duration of the pore opening (~10 min) should be sufficient for CTB to access the entire vesicle interior (as explained below), while at the same time desorption of GM1 from the membrane should be negligible as it is slow (32). To a good approximation, the diffusion coefficient, D, of CTB is on the order of 60 $\mu m^2/s$ or higher [taking ~4 nm for the hydrodynamic radius of CTB (33)], suggesting that within a couple of seconds CTB will explore a distance, L, comparable to the vesicle size: $L = \sqrt{2dDt} > 20 \mu \text{m}$, where d = 3 is dimensionality and t is time. Indeed, time-lap observations suggest that the fluorescence signal from CTB-Alexa saturates already in the first couple of seconds after the pore opens (SI Appendix, Fig. S3B).

To estimate the ratio of GM1 coverage in the membrane leaflets, we plotted the mean intensity across the membrane before and after poration (the signal was averaged over many line scans across the vesicle membrane from different confocal sections following an approach in ref. 34) (Fig. 2D and SI Appendix, section S4). A twofold signal increase signifies symmetric distribution of GM1 between the inner and outer leaflets, as demonstrated on the symmetric membranes (SI Appendix, section S4). Higher signal indicates a higher concentration of GM1 in the inner leaflet, while lower signal would suggest the opposite. The intensity profiles measured across the membrane have a ratio of the integrated peak areas equal to ~4.73. This indicates predominant localization of GM1 in the inner leaflet.

Because the partitioning coefficient of GM1 between the membrane and the bulk (inside and outside the vesicles) is the same before and after dilution, one can roughly estimate the molar concentrations of the ganglioside present in the inner and outer leaflets taking into account the total lipid concentration in the samples (*SI Appendix*, section S5). Table 1 shows results for the

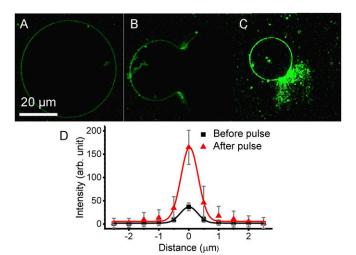


Fig. 2. Electroporation assay for assessing the asymmetric distribution of GM1 between the membrane leaflets. (A) Confocal image of a vesicle prepared with 4 mol% GM1 and incubated with CTB-Alexa (green), which binds to GM1 located only in the outer leaflet of the membrane. (B) Electroporation of the vesicle using a DC pulse (10 kV/m, 50 ms). The large pore allows binding of CTB to GM1 present also in the inner leaflet of the membrane. (C) The fluorescence intensity quickly attains a steady value, and after about 10 min, the vesicle membrane closes to form a smaller vesicle. All images in A-C were recorded for the same setting of the microscope and processed in the same way. (D) Intensity profiles across the membrane averaged over the circular part of the membrane contour before (A) and after poration (C) (SI Appendix, section S4). The solid curves are Gaussian fits. Errors have been estimated as SD of values along the vesicle contour.

fractions of GM1 with respect to the total number of lipids in the inner and outer leaflets, ϕ_{in} and ϕ_{out} , respectively. The SE from measurements on different vesicles is of the order of 14% (six vesicles with 4 mol% GM1 and five vesicles with 2 mol% GM1 were examined). The measurements were performed at room temperature; therefore, high GM1 fractions, at which the membrane undergoes phase separation (25), were not explored.

A Method to Measure the Membrane Spontaneous Curvature. Tomeasure the spontaneous curvature of these asymmetric membranes, we developed a technique based on pulling inward and outward tubes. The experimental assay combines a micropipette for aspirating GUVs and optical tweezers to extrude a membrane tube as shown in Fig. 3. The setup can simultaneously measure the force acting on the tube, perform epifluorescence imaging, and control membrane tension via micropipette aspiration (SI Appendix, sections S6 and S7; Materials and Methods). By varying the aspiration pressure in the micropipette, one changes the membrane tension of the GUV. A latex sphere attached to the GUV membrane is trapped using the optical tweezers and manipulated to the GUV and away from the membrane to form membrane tubes both inwardly as well as outwardly (SI Appendix, section S8). Outward tubes with similar setups have been pulled by several groups (see, e.g., refs. 23 and 35-37). Pulling inward tubes has been established only recently (38) whereby hydrodynamic forces were employed. Here, we combine the two approaches to assess membrane material properties such as the spontaneous curvature and bending rigidity. We also demonstrate that to assess the spontaneous curvature, no prior knowledge of the membrane tension is needed as long as outward and inward tubes are pulled on the same vesicle.

To analyze the shape of the GUVs in Fig. 3 A and B, we distinguish three membrane segments: the small spherical segment within the pipette, which has the radius R_{pip} ; the large spherical segment outside of the pipette, which has the radius $R_{\rm sp}$; and the pulled nanotube, which we take to be cylindrical with radius R_{tu} . We now assume that the vesicle membrane is uniform in the sense that all of these membrane segments have the same spontaneous curvature m and the same bending rigidity κ . The small spherical segment, which is exposed to the pressure difference $P_{\rm in} - P_{\rm pip}$, is then governed by the shape equation

$$P_{\rm in} - P_{\rm pip} = 2(\Sigma + 2\kappa m^2) \frac{1}{R_{\rm pip}} - 4\kappa m \frac{1}{R_{\rm pip}^2},$$
 [1]

which also depends on the mechanical tension Σ and on the spontaneous tension $2\kappa m^2$. The large spherical segment is exposed to the pressure difference $P_{\rm in} - P_{\rm ex}$, and its radius $R_{\rm sp}$ satisfies the shape equation

$$P_{\rm in} - P_{\rm ex} = 2(\Sigma + 2\kappa m^2) \frac{1}{R_{\rm sp}} - 4\kappa m \frac{1}{R_{\rm sp}^2}.$$
 [2]

Combining these two equations, we obtain the suction pressure

$$\Delta P = P_{\text{ex}} - P_{\text{pip}} \approx 2\left(\Sigma + 2\kappa m^2\right) \left(\frac{1}{R_{\text{pip}}} - \frac{1}{R_{\text{sp}}}\right),$$
 [3]

where correction terms of order $m/R_{\rm pip}^2$ and $m/R_{\rm sp}^2$ have been ignored. When we rearrange the terms in the latter equation, we obtain the relation

$$\Sigma + 2\kappa m^2 \approx \Delta P \frac{R_{\rm sp} R_{\rm pip}}{2(R_{\rm sp} - R_{\rm pip})} \equiv \Sigma_{\rm asp},$$
 [4]

which defines the aspiration tension Σ_{asp} . Thus, up to this order, the total membrane tension,

$$\hat{\Sigma} \equiv \Sigma + 2\kappa m^2,$$
 [5]

is equal to the aspiration tension Σ_{asp} , which can be controlled via the suction pressure ΔP .

The out-tube with positive mean curvature is exposed both to the pressure difference $P_{\rm in}$ – $P_{\rm ex}$ and to the local pulling force f_{out} . Likewise, the in-tube with negative mean curvature is

Table 1. Molar fractions of GM1 in the inner and outer leaflets, ϕ_{in} and ϕ_{out} , and membrane spontaneous curvature

	Intensity ratio		raction ol%	Asymmetry, $\Delta \phi = \phi_{\rm in} - \phi_{\rm out}$, mol%	Spontaneous curvature m^{-1} , nm	
Total mol% GM1	$I_{\text{after}}/I_{\text{before}}$	ϕ_{in}	ϕ_{out}		Out-tubes	In-tubes
2	5.19	1.98	0.47	1.51	-510 ± 142	-411 ± 110
4	4.73	3.97	1.07	2.90	-235 ± 45	−213 ± 29

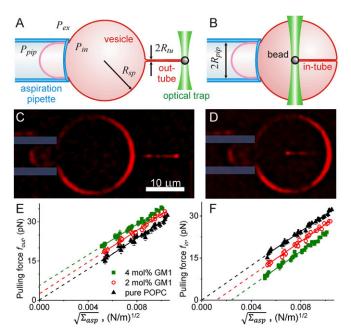


Fig. 3. Experimental assay for measuring spontaneous curvature and bending rigidity. The vesicle membrane tension $\Sigma_{\rm asp}$ is set by the suction pressure of the micropipette. A membrane-bound bead is trapped with optical tweezers to pull membrane tubes from the aspirated vesicle either (A and C) outwardly or (B and D) inwardly. The tubes can be observed with epifluorescence (C and D): for these examples, the aspirated vesicle (labeled with 0.1 mol% TR-DHPE) is held at aspiration pressure corresponding to $\sim\!0.01$ mN/m. Fourier filtering has been aspiration pressure corresponding to mentubes. The plots of force versus $\sqrt{\Sigma_{\rm asp}}$ for vesicles prepared with varying GM1 concentrations are given for outward (E) and inward (F) tubes. The same vesicles were used for pulling in-tubes and out-tubes. The data are collected from five vesicles for each membrane composition. The solid lines are fits following Eqs. 6 and 7. The intercepts with the y axis can be used to deduce the membrane spontaneous curvature following Eq. 9.

exposed both to $P_{\rm in}$ – $P_{\rm ex}$ and $f_{\rm in}$. Using the results of ref. 39, we obtain the equations

$$f_{\rm in} = 2\pi \sqrt{2\kappa(\Sigma + 2\kappa m^2)} + 4\pi\kappa m \approx 2\pi \sqrt{2\kappa\Sigma_{\rm asp}} + 4\pi\kappa m$$
 [6]

for in-tubes, and

$$f_{\rm out} = 2\pi \sqrt{2\kappa(\Sigma + 2\kappa m^2)} - 4\pi\kappa m \approx 2\pi \sqrt{2\kappa\Sigma_{\rm asp}} - 4\pi\kappa m$$
 [7]

for out-tubes. Therefore, for m < 0, the force f_{in} vanishes at

$$\Sigma_{\rm asp}^0 = 2\kappa m^2$$
 forin-tubes, [8]

which represents the spontaneous tension generated by the spontaneous curvature. For out-tubes and in-tubes, the pulling forces at vanishing tension are given by

$$f_{\text{out}}^0 = -4\pi\kappa m$$
 and $f_{\text{in}}^0 = 4\pi\kappa m$. [9]

From Eqs. 6 and 7, one also sees that pulling an in-tube and an out-tube and measuring the respective forces at a fixed membrane tension allows us to directly estimate the spontaneous curvature from the force difference, $f_{\text{out}} - f_{\text{in}} = -8\pi\kappa m$, which does not depend on the membrane tension (*SI Appendix*, Fig. S5) as we confirm experimentally below on vesicles aspirated in micropipettes. Thus, no prior knowledge of the membrane tension is needed. Therefore, as long as the vesicle is immobilized (for example by adhesion to a substrate), such measurements can be performed on nonaspirated vesicles, avoiding the need of having a

complex micropipette aspiration setup. The only condition is that the unbound part of the vesicle retains its spherical cap morphology and the pulling of in- and out-tubes does not perturb it.

The tube pulling force was studied in vesicles prepared with varying concentrations of GM1. Both an in-tube and an out-tube were pulled from the same vesicle and the forces were measured under changing membrane tension. Fig. 3 E and F shows the tube pulling force with increasing tension. The slope of linear fits following Eqs. 6 and 7 provides an estimate for the bending modulus, whereby the value obtained from inward tubes ($\kappa = 1.20 \pm 0.07 \times 10^{-19}$ J) is consistent with that from outward tubes ($\kappa = 1.10 \pm 0.11 \times 10^{-19}$ J); every vesicle was analyzed independently, and then the results were averaged; the error represents the maximal error from individual vesicle fits. This value is also consistent with literature data for POPC membranes (40). It is relatively constant over samples with and without GM1 and varies within 10%, which is comparable to the measurement errors for the present experiments as well as that of the electroporation experiments for assessing the GM1 distribution. One may expect a decrease in the bending stiffness of the vesicle membrane with the addition of GM1 as reported in ref. 25; however, in the latter study, the GM1 concentration on the membrane was higher as no dilution of the vesicles was done (i.e., no significant desorption of GM1 occurred).

The linear fits to the data for pure POPC vesicles in Fig. 3 E and F go through the origin. This is understandable as these membranes exhibit no asymmetry and thus have zero spontaneous curvature (Eq. 9). For vesicles prepared with GM1, the intercept of the fits is positive for outward tubes and negative for inward tubes consistent with a negative value for the membrane spontaneous curvature resulting from the asymmetric distribution of GM1. The membrane curvatures m^{-1} estimated from the intercepts (Eq. 9) for in-tubes are consistent with values obtained from pulling out-tubes (Table 1). With increasing GM1 concentration, higher forces are required to pull outward membrane tubes at a given tension (Fig. 3E). Simultaneously, the inward tube pulling force vanishes at higher values of $\Sigma^0_{\rm asp}$ (Fig. 3F and Eq. 8). This implies that at higher concentrations of GM1 in the membrane, spontaneously formed tubes will be stable even at higher aspiration tension applied on the vesicle. Indeed, this result was found consistent with another set of experiments for higher GM1 fractions, where we explored the threshold membrane tension below which tubes spontaneously reform (for details, see SI Appendix, section S9). A similar approach was previously applied to another system (see ref. 41). Here, the membrane tension was modulated either via micropipette aspiration or vesicle electrodeformation (25, 42). The threshold membrane tension was observed to increase up to around 0.025 mN/m for membranes prepared with 10 mol% GM1 (SI Appendix, Fig. S6).

Comparison with Simulations: Independence of Membrane Mechanical Properties on Local Clustering of GM1. We performed simulations using the MARTINI coarse-grained molecular-dynamics simulation model with a GM1 parameterization that combines the bonded parameters by López et al. (43) with the nonbonded parameters by Gu et al. (44) (Fig. 4A, Materials and Methods, and SI Appendix, section S10). The effect of GM1 on the bilayer spontaneous curvature as assessed from the first moment of the stress profile, which is equal to $-2\kappa m$, is shown in Fig. 4B as a function of the bilayer asymmetry $\phi_{\rm in} - \phi_{\rm out}$, where $\phi_{\rm in}$ and $\phi_{\rm out}$ are the mole fractions of GM1 in the inner and the outer leaflet. For comparison, experimental data as deduced from the measured pulling force for vanishing tension (Eq. 9 and Table 1) are also plotted in Fig. 4B. The simulations showed an overall negative spontaneous curvature for the range of studied asymmetry values, consistent with the experimental data. Interestingly, the simulation data are well fitted by a straight line in agreement with theoretical predictions (39). Note that the fit shown in Fig. 4B (dashed line) was obtained for the simulation data with $\phi_{\rm out} = 0$, that is, when the outer leaflet contained pure POPC, but simulation data with $\phi_{\rm out} = 1$, that is, when the outer leaflet contained a single GM1 followed the same dependence on bilayer asymmetry. Furthermore, this linear relation captured also the dependence of our experimental data quantitatively. The original model by López et al. (43) also captured the experimental data quantitatively (SI Appendix, Fig. S8), despite the fact that this model suffers from unphysically strong GM1 clustering [see Gu et al. (44) and SI Appendix, Figs. S7A and S8A]. As our model reproduces all of the other properties [including the GM1 shape (SI Appendix, Fig. S7B)] of the López model except for the clustering, our simulation results demonstrate that the effect GM1 has on the membrane mechanical properties (Fig. 4B and SI Appendix, Fig. S8B) is, interestingly, independent of the local clustering of GM1.

Estimate for Local Curvature Generated by GM1. The spontaneous tension generated by the tubes, Σ_{asp}^0 , and the pulling forces at vanishing tension, f_{out}^0 and f_{in}^0 , can be used to obtain an estimate for the local curvature generated by a single GM1, \tilde{m} , via the relation $m = \Delta \phi \alpha \tilde{m}$, where $\Delta \phi = \phi_{\rm in} - \phi_{\rm out}$ represents the membrane asymmetry deduced from the electroporation assay (Table 1), and α is a correction factor accounting for the molecular surface areas of GM1 and POPC, $\alpha = a_{\rm GM1}/a_{\rm POPC}$. The average bilayer area occupied by the GM1 molecule is reported to be between 70 and 85 Å² (45), that is, $a_{\rm GM1} \cong 77$ Å², while that of POPC is $a_{\rm POPC} \cong 63$ Å² (46), yielding $\alpha \cong 1.2$. Second-order curves for the dependence of $\Sigma^0_{\rm asp}$ on $\Delta \phi$ for vesicles prepared from pure POPC ($\Delta \phi = 0$) and with 2 and 4 mol% GM1 give $\tilde{m}^{-1} = 7.38 \pm 1.49$ nm for data from pulled in-tubes. Linear fits of the out-tube and in-tube pulling forces at vanishing tension as a function of $\Delta \phi$ yield $\tilde{m}^{-1} = 8.07 \pm 1.74$ nm. These results are in excellent agreement. The combined results for the local curvature generated by GM1 in POPC membranes lead to $\tilde{m}^{-1} = 7.73 \pm 1.62$ nm. Alternatively, the projected membrane surface area under a GM1 head group can be assessed from simulation data yielding $\alpha_{\text{sim}} \cong 2$ and, correspondingly, $\tilde{m}_{\text{sim}}^{-1} = 12.56 \pm 0.50$ nm. It is pertinent to note here that \tilde{m} is the local curvature generated by GM1 molecules in bilayer membranes and represents a molecular characteristic. For comparison, in lipid-free systems, as examined extensively in the past, it can be estimated from the radius of GM1 micelles. Sonnino et al. (47) have reported a hydrodynamic radius of ~5.87 nm for GM1 micelles. Note, however, that in micelles, the molecular environment of the molecule is very different compared with that in the lipid bilayer.

Conclusions

The involvement of gangliosides in important cellular processes like neuronal functioning is now well known, and the curvature properties of these glycosphingolipids play a crucial role in axonal sprouting and important neuron repair processes. We have used an optical-tweezers-based approach to pull thin tubes from giant vesicles made with GM1 lipids and studied the tube pulling force to obtain a fairly accurate estimate of the spontaneous curvature generated by GM1 molecules. Since an important aspect of curvature-inducing characteristic of GM1 is its localization primarily on one leaflet of cell membranes, we prepared vesicles with asymmetric GM1 distribution across the bilayer. This was achieved based on our finding that GM1 desorbs from the membrane. One important practical aspect to emphasize here is that the large number of studies based on using model and cell membranes containing GM1 should consider the desorption aspects ensuing from sample dilution to allow for data comparison across laboratories and for appropriate interpretation of results (especially when membrane morphology is studied). The dilution steps will presumably alter the affinity of GM1-doped membranes to various receptors. Here, we quantified GM1 desorption and the resulting leaflet asymmetry by an approach involving generation of transient pores in giant vesicles by electroporation. We also determined the dependence of the membrane spontaneous curvature on GM1 asymmetry. Coarse-grained moleculardynamics simulations captured the experimentally obtained data

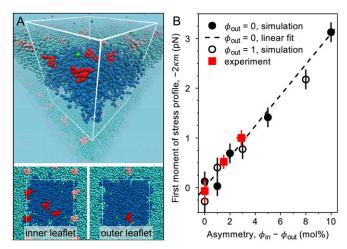


Fig. 4. Simulation results and comparison with experiment. (A) A simulation snapshot of the inner bilayer leaflet (upper monolayer within the white wireframe) and the outer leaflet (lower monolayer) for GM1 molar fractions $\phi_{\rm in}$ = 4 mol% and $\phi_{\rm out}$ = 1 mol% using the MARTINI coarse-grained moleculardynamics simulation model with GM1 parameters developed in this work by combining the bonded parameters by López et al. (43) with the nonbonded parameters by Gu et al. (44). Leaflet-wise mole fractions directly indicate the numbers of lipids: $\phi_{in} = 4$ corresponds to 4 GM1 and 96 POPC molecules in the inner leaflet. The white wire frame with the strongly colored species (GM1, red; POPC, blue; sodium, green; water, not shown) shows the simulation box, and the lightly colored molecules indicate its periodic images. (B) Comparison of simulation results to experiments. The first moment of the lateral stress profile (–2 κm) is plotted as a function of the bilayer asymmetry $\phi_{\rm in}$ – $\phi_{\rm out}$ for bilayers when the outer leaflet is pure POPC ($\phi_{\rm out}$ = 0, solid circles), and when it contains one GM1 ($\phi_{\rm out}$ = 1, open circles). Error bars indicate SEM. The dashed line represents the linear fit $-2\kappa m = 0.31(\phi_{\rm in} - \phi_{\rm out})$ to the data for $\phi_{\rm out} = 0.31(\phi_{\rm in} - \phi_{\rm out})$ The dependence is quantitatively consistent with the experimental results (red squares) obtained from the pulling force for vanishing tension (Eq. 9).

quantitatively correctly and showed that the effect of GM1 on bilayer mechanical properties does not depend on the local clustering of GM1. We expect our GM1 model to have the predictive power for assessing the membrane curvature at higher asymmetries, characteristic for neuronal membranes. However, we expect that this predictive ability is sensitive to the details of the parameterization and that future studies will allow us to bring light to the importance of head group orientation on the ability of GM1 (and glycolipids in general) to modify membrane mechanical properties. The multitasking role of GM1 and its involvement in a large number of essential functions in the membrane has been well recognized, in particular, its involvement in neuronal development and differentiation (48, 49) and neurite sprouting (50). Our results on curvature generation of GM1 point to an additional important role of this ganglioside, namely, shaping neuronal membranes.

Materials and Methods

Vesicle Preparation. GUVs were grown in 1 mM Hepes using the electroformation technique from a mixture of ~3 mM POPC and GM1 with varying concentration of up to 10 mol% of the total lipid content (25) (SI Appendix, section S1). For fluorescence imaging of the vesicles, 0.1 mol% Texas Red dihexadecanoyl-glycerophosphoethanolamine (TR-DHPE) or 0.1 mol% BODIPY FL C5-ganglioside GM1 (BODIPY-GM1) was added. Occasionally, CTB labeled with Alexa 488 (CTB-Alexa) (purchased from Invitrogen) was added, and the vesicles were imaged with a confocal microscope (SP5 DMI 6000: Leica Microsystems).

Optical Tweezers and Force Measurements. The optical tweezers were built around a motorized inverted microscope (Axiovert 200M; Zeiss) by focusing a 1,064-nm, continuous-wave beam from a Nd:YAG laser through a 100x, 1.25 N.A. objective lens (51). The bead position was determined using centroid tracking algorithm (52). The trap stiffness of the tweezers was found to be typically ~110 pN/μm/W (SI Appendix, section S6). All force-measurement experiments were performed at room temperature, 23 \pm 1 °C.

Micropipette Manipulation and Aspiration of GUVs. Micropipettes were fashioned from glass capillaries at desired inner diameters of \sim 6 μ m. The aspiration pressure was controlled through movement of a water reservoir. More details on the vesicle micromanipulation procedure are given in *SI Appendix*, sections S7 and S8.

Coarse-Grained Molecular-Dynamics Simulations. We used the fast, flexible, and free GROMACS (53) engine, version 5.1.1, to run MARTINI (54) coarse-grained molecular-dynamics simulations (*SI Appendix*, section \$10). The GM1-containing POPC bilayers at full hydration (at least 15 water beads, equivalent of 60 water molecules, per lipid), were simulated using a GM1 parameterization that combined the bonded parameters in ref. 43, with

- 1. Sonnino S, Mauri L, Chigorno V, Prinetti A (2007) Gangliosides as components of lipid membrane domains. *Glycobiology* 17:1R–13R.
- Cantù L, Corti M, Brocca P, Del Favero E (2009) Structural aspects of gangliosidecontaining membranes. Biochim Biophys Acta 1788:202–208.
- Klenk E (1939–1940) Beiträge zur Chemie der Lipoidosen. Hoppe Seylers Z Physiol Chem 262:128–144.
- Yu RK, Tsai YT, Ariga T (2012) Functional roles of gangliosides in neurodevelopment: An overview of recent advances. Neurochem Res 37:1230–1244.
- Skaper SD, Katoh-Semba R, Varon S (1985) GM1 ganglioside accelerates neurite outgrowth from primary peripheral and central neurons under selected culture conditions. Brain Res 355:19–26.
- Kabaso D, Lokar M, Kralj-Iglič V, Veranič P, Iglič A (2011) Temperature and cholera toxin B are factors that influence formation of membrane nanotubes in RT4 and T24 urothelial cancer cell lines. *Int J Nanomedicine* 6:495–509.
- Lou E, et al. (2012) Tunneling nanotubes provide a unique conduit for intercellular transfer of cellular contents in human malignant pleural mesothelioma. PLoS One 7: e33093.
- Callan-Jones A, Bassereau P (2013) Curvature-driven membrane lipid and protein distribution. Curr Opin Solid State Mater Sci 17:143–150.
- Callan-Jones A, Sorre B, Bassereau P (2011) Curvature-driven lipid sorting in biomembranes. Cold Spring Harb Perspect Biol 3:a004648.
- Yamakawa T, Nagai Y (1978) Glycolipids at the cell surface and their biological functions. Trends Biochem Sci 3:128–131.
- Bacia K, Scherfeld D, Kahya N, Schwille P (2004) Fluorescence correlation spectroscopy relates rafts in model and native membranes. Biophys J 87:1034–1043.
- Bacia K, Schwille P, Kurzchalia T (2005) Sterol structure determines the separation of phases and the curvature of the liquid-ordered phase in model membranes. Proc Natl Acad Sci USA 102:3272–3277.
- Römer W, et al. (2007) Shiga toxin induces tubular membrane invaginations for its uptake into cells. Nature 450:670–675.
- Ewers H, et al. (2010) GM1 structure determines SV40-induced membrane invacination and infection. Nat Cell Biol 12:11–18.
- Ewers H, Helenius A (2011) Lipid-mediated endocytosis. Cold Spring Harb Perspect Biol 3:a004721.
- 16. Rissanen S, et al. (2017) Phase partitioning of GM1 and its bodipy-labeled analog determine their different binding to cholera toxin. Front Physiol 8:252.
- 17. Hägerstrand H, et al. (2006) Curvature-dependent lateral distribution of raft markers in the human erythrocyte membrane. *Mol Membr Biol* 23:277–288.
- 18. Mukherjee S, Maxfield FR (2000) Role of membrane organization and membrane
- domains in endocytic lipid trafficking. *Traffic* 1:203–211.

 19. Mukherjee S, Soe TT, Maxfield FR (1999) Endocytic sorting of lipid analogues differing
- Mukherjee S, Soe LL, MaxTield FK (1999) Endocytic Sorting of lipid analogues differing solely in the chemistry of their hydrophobic tails. J Cell Biol 144:1271–1284.
 Markin VS (1981) Lateral organization of membranes and cell shapes. Biophys J 36:
- 1–19.21. Seifert U (1993) Curvature-induced lateral phase segregation in two-component
- vesicles. *Phys Rev Lett* 70:1335–1338.

 22. Fournier JB (1996) Nontopological saddle-splay and curvature instabilities from an-
- isotropic membrane inclusions. *Phys Rev Lett* 76:4436–4439.

 23. Sorre B, et al. (2009) Curvature-driven lipid sorting needs proximity to a demixing
- point and is aided by proteins. *Proc Natl Acad Sci USA* 106:5622–5626.

 24. Ramesh P, et al. (2013) FBAR syndapin 1 recognizes and stabilizes highly curved tu-
- Kamesn P, et al. (2013) FBAK syndapin 1 recognizes and stabilizes highly curved tubular membranes in a concentration dependent manner. Sci Rep 3:1565.
 Fricke N, Dimova R (2016) GM1 softens POPC membranes and induces the formation
- of micron-sized domains. *Biophys J* 111:1935–1945.

 26. Yuan C, Johnston LJ (2001) Atomic force microscopy studies of ganglioside
- Yuan C, Johnston LJ (2001) Atomic force microscopy studies of ganglioside GM1 domains in phosphatidylcholine and phosphatidylcholine/cholesterol bilayers. Biophys J 81:1059–1069.
- Liu Y, Agudo-Canalejo J, Grafmüller A, Dimova R, Lipowsky R (2016) Patterns of flexible nanotubes formed by liquid-ordered and liquid-disordered membranes. ACS Nano 10:463–474.
- Riske KA, Dimova R (2005) Electro-deformation and poration of giant vesicles viewed with high temporal resolution. *Biophys J* 88:1143–1155.
- Portet T, Dimova R (2010) A new method for measuring edge tensions and stability of lipid bilayers: Effect of membrane composition. *Biophys J* 99:3264–3273.
- 30. Dimova R, et al. (2009) Vesicles in electric fields: Some novel aspects of membrane behavior. *Soft Matter* 5:3201–3212.

the nonbonded parameters in ref. 44, see *SI Appendix*, section S10. The lateral stress profiles of the bilayers were calculated with GROMACS-LS (55). The simulation lengths were 100 μ s (except for the $\phi_{in}|\phi_{out}=1|1$ system, 20 μ s) with sampling rate of 100 ps.

Note Added in Proof. Bhatia et al. (56) have recently determined the spontaneous curvature of GUVs doped with GM1 by an alternative method.

ACKNOWLEDGMENTS. We acknowledge Y. Liu for help with the code for analyzing the intensity line profiles across the membrane. This work is part of the MaxSynBio Consortium, which is jointly funded by the Federal Ministry of Education and Research of Germany and the Max Planck Society.

- 31. Dimova R, et al. (2007) Giant vesicles in electric fields. Soft Matter 3:817-827.
- Masserini M, Freire E (1987) Kinetics of ganglioside transfer between liposomal and synaptosomal membranes. Biochemistry 26:237–242.
- Miller CE, Majewski J, Watkins EB, Weygand M, Kuhl TL (2008) Part II: Diffraction from two-dimensional cholera toxin crystals bound to their receptors in a lipid monolayer. *Biophys J* 95:641–647.
- Pataraia S, Liu Y, Lipowsky R, Dimova R (2014) Effect of cytochrome c on the phase behavior of charged multicomponent lipid membranes. *Biochim Biophys Acta* 1838: 2036–2045.
- Capraro BR, Yoon Y, Cho W, Baumgart T (2010) Curvature sensing by the epsin Nterminal homology domain measured on cylindrical lipid membrane tethers. J Am Chem Soc 132:1200–1201.
- Heinrich M, Tian A, Esposito C, Baumgart T (2010) Dynamic sorting of lipids and proteins in membrane tubes with a moving phase boundary. Proc Natl Acad Sci USA 107:7208–7213.
- Sorre B, et al. (2012) Nature of curvature coupling of amphiphysin with membranes depends on its bound density. Proc Natl Acad Sci USA 109:173–178.
- Dasgupta R, Dimova R (2014) Inward and outward membrane tubes pulled from giant vesicles. J Phys D Appl Phys 47:282001.
- Lipowsky R (2013) Spontaneous tubulation of membranes and vesicles reveals membrane tension generated by spontaneous curvature. Faraday Discuss 161: 305–331. discussion 419–459.
- 40. Dimova R (2014) Recent developments in the field of bending rigidity measurements on membranes. Adv Colloid Interface Sci 208:225–234.
- Li Y, Lipowsky R, Dimova R (2011) Membrane nanotubes induced by aqueous phase separation and stabilized by spontaneous curvature. Proc Natl Acad Sci USA 108: 4721–4736
- Gracià RS, Bezlyepkina N, Knorr RL, Lipowsky R, Dimova R (2010) Effect of cholesterol
 on the rigidity of saturated and unsaturated membranes: Fluctuation and electrodeformation analysis of giant vesicles. Soft Matter 6:1472–1482.
- López CA, Sovova Z, van Eerden FJ, de Vries AH, Marrink SJ (2013) Martini force field parameters for glycolipids. J Chem Theory Comput 9:1694–1708.
- Gu R-X, Ingólfsson HI, de Vries AH, Marrink SJ, Tieleman DP (2017) Ganglioside-lipid and ganglioside-protein interactions revealed by coarse-grained and atomistic molecular dynamics simulations. J Phys Chem B 121:3262–3275.
- Maggio B (1994) The surface behavior of glycosphingolipids in biomembranes: A new frontier of molecular ecology. Proa Biophys Mol Biol 62:55–117.
- Kučerka N, Nieh MP, Katsaras J (2011) Fluid phase lipid areas and bilayer thicknesses
 of commonly used phosphatidylcholines as a function of temperature. Biochim
 Biophys Acta 1808:2761–2771.
- 47. Sonnino S, Cantù L, Corti M, Acquotti D, Venerando B (1994) Aggregative properties of gangliosides in solution. *Chem Phys Lipids* 71:21–45.
- Skaper SD, Leon A, Toffano G (1989) Ganglioside function in the development and repair of the nervous system. From basic science to clinical application. Mol Neurobiol 3:173–199.
- 49. Ledeen RW, Wu G (2015) The multi-tasked life of GM1 ganglioside, a true factotum of nature. *Trends Biochem Sci* 40:407–418.
- Roisen FJ, Bartfeld H, Nagele R, Yorke G (1981) Ganglioside stimulation of axonal sprouting in vitro. Science 214:577–578.
- Kraikivski P, Pouligny B, Dimova R (2006) Implementing both short- and long-working-distance optical trappings into a commercial microscope. Rev Sci Instrum 77: 113703.
- 52. Dasgupta R, Verma RS, Gupta PK (2012) Microfluidic sorting with blinking optical traps. *Opt Lett* 37:1739–1741.
- Abraham MJ, et al. (2015) GROMACS: High performance molecular simulations through multi-level parallelism from laptops to supercomputers. SoftwareX 1-2: 19–25.
- Marrink SJ, Risselada HJ, Yefimov S, Tieleman DP, de Vries AH (2007) The MARTINI force field: Coarse grained model for biomolecular simulations. J Phys Chem B 111: 7812–7824.
- Vanegas JM, Torres-Sánchez A, Arroyo M (2014) Importance of force decomposition for local stress calculations in biomembrane molecular simulations. J Chem Theory Comput 10:691–702.
- Bhatia T, Agudo-Canalejo J, Dimova R, Lipowsky R (April 16, 2018) Membrane nanotubes increase the robustness of giant vesicles. ACS Nano, 10.1021/acsnano.8b00640.

Supporting Information

The reshaping role of GM1: membrane curvature and asymmetry in giant vesicles

Raktim Dasgupta^{1,2}, Markus S. Miettinen¹, Nico Fricke^{1,3}, Reinhard Lipowsky¹ and Rumiana Dimova^{1,*}

Text S1. Preparation of giant unilamellar vesicles (GUVs)

GUVs were grown using the electroformation technique (1). 1-palmitoyl-2-oleoyl-snglycero-3-phosphatidylcholine (POPC) and GM1 with varying concentration of up to 10 mol% were dissolved in a dichloromethane:methanol (2:1) solution to a concentration of 3.19 mM. Both lipids were purchased from Avanti Polar Lipids (Alabaster, AL). For fluorescence imaging of the vesicles, additionally 0.1 mol% Texas Red dihexadecanoylglycerophosphoethanolamine (TR-DHPE) or 0.1 mol% Bodipy FL C5-ganglioside GM1 (Bodipy-GM1) were added. 20 µl of the lipid solution was spread onto the electrically conductive sides of two indium-tin oxide (ITO)-coated glass plates (Delta technologies Lt.) heated to 50 °C and dried under vacuum for two hours to remove the organic solvents. The glass plates were put against a 2 mm thick Teflon spacer to form a close chamber. 1 mM HEPES buffer (pH 7.4, 0.5 Na HEPES; Sigma-Aldrich, St. Louis, MO) was filled into the chamber and thereafter a sinusoidal AC electric field at 10 Hz was applied for electroswelling the lipid films. In the first phase of the electroswelling process, the amplitude of the applied field was linearly increased from 0.1 V (peak to peak) to 0.8 V (peak to peak) over 30 min. Thereafter the voltage was held steady for 60 min for growing the vesicles. Detachment of the formed vesicles from the glass surfaces was achieved by subsequent application of electric field with decreasing frequency down to 5 Hz over 20 minutes. All the voltages were

¹ Department of Theory and Bio-Systems, Max Planck Institute of Colloids and Interfaces, Science Park Golm, 14424 Potsdam, Germany

² Current address: Laser Biomedical Applications Section, Raja Ramanna Centre for Advanced Technology, Indore-452013, India

³ Current address: Department of Molecular Physiology and Biophysics, Vanderbilt University, School of Medicine, Nashville, Tennessee (TN)

^{*}E-mail: dimova@mpikg.mpg.de

measured at the ITO coated glass plates. Once the vesicles are formed, they were found to be stable and could be transferred to glass chambers used under microscopes for further investigations. Both the drying and electroswelling were carried out at 40 °C since at that temperature the lipid bilayer remains fluid and no phase separation occurs (2).

Text S2. Internal tubes generated upon dilution of vesicle suspensions

To understand the origin of the asymmetric distribution of GM1 across the membrane bilayer we carried out studies on the vesicles at different stages of preparation. The vesicle electroformation was performed under the confocal microscope while keeping the temperature of the solution constant at about 40 °C by placing the electroformation chamber in contact with a heat-flow chamber connected to a thermostat. Electroformed vesicles either attached to the glass substrate or floating were observed, but none of these could be seen with internal tubes (Fig. S1A). Since during electroformation the vesicle membrane tension remains high and this could be a likely reason for not observing any tubes, after electroformation, the vesicle suspension was transferred to a glass container and kept at room temperature overnight so that the vesicles could relax. Similar observations were made whereby only occasional vesicles could be found with internal tubes. The majority of the vesicles were free of tubes (Fig. S1B). Finally, the vesicle solution was diluted tenfold in a freshly prepared 1 mM HEPES buffer. Soon after that, a large number of vesicles with internal tubes could be seen (Fig. S1C). The observation suggests the important role of dilution of the vesicle external medium by vesicle-free buffer in the occurrence of the tubes.

To understand whether using HEPES as dilution medium is the key factor in the tube formation process, we also prepared vesicles in pure water. The observations were identical as with HEPES and shown in Fig. S1D,E. Minimal tube formation was observed until the original suspension medium was tenfold diluted by fresh water (Fig. S1E). This clearly suggests that the tube formation mechanism is independent of HEPES being used as suspension medium and dependent on the dilution of the concentration of GM1 in the surrounding medium of the prepared vesicles.

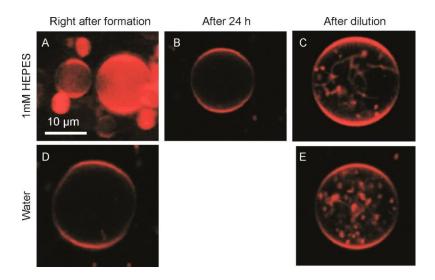


Figure S1. Vesicles observed at different stages of preparation in (A-C) 1 mM HEPES solution or (D, E) water. Internal tubes are observed only after the surrounding medium of the vesicles were diluted tenfold by fresh medium, i.e. HEPES buffer or water (C, E).

S3. Generation of external tubes upon external addition of GM1

The formation of internal nanotubes in the GM1 doped vesicles upon dilution of the external medium indicates desorption of GM1 from the outer leaflet leading to an asymmetric distribution of GM1 between the leaflets. To confirm this, we carried out the following experiment. In the diluted suspension of vesicles, when the internal nanotubes are formed, GM1 was added to the external medium to increase the concentration of GM1 in the outer leaflet by spontaneous insertion of the molecules at higher surrounding concentrations. A simple estimate for vesicles prepared with 4 mol% GM1 used in the total lipid mixture and assuming that all of the lipid and GM1 has been included either in the solution or in the form of vesicles, the total concentration of GM1 after dilution with fresh buffer comes out to be about 1.45×10⁻⁷ M. This concentration includes GM1 which is membrane-bound as well as dissolved in the medium. Taking half of the above concentration as the upper limit for GM1 present in the inner leaflet, we added ~0.73×10⁻⁷ M GM1 (6 µl of 1.28×10⁻⁵ M GM1 dissolved in dichloromethane/methanol (2:1) solution) from outside to adjust the concentration of GM1 in the exterior medium to be the same or higher. Leaving the vesicle solution open for about 10 minutes let the small amount of methanol/dichloromethane mixture (added with GM1) evaporate and thereafter observations were made on the vesicles. Although some vesicles appeared to be damaged because of the addition of methanol/dichloromethane mixture, a large fraction of undamaged vesicles were observed to

attain a balanced distribution of GM1 between the two leaflets as judging from their smooth appearance without any internal tubes. More interestingly, occasionally some vesicles even with long external tubes could be seen. The occurrence of external tubes indicates higher concentration of GM1 in the outer leaflet of these vesicles and presumably results from the inhomogeneous distribution of GM1 following the addition. Note that the addition of the same amount of GM1-free methanol/dichloromethane solution did not lead to suppression of the internal tubes, but only resulted in rupturing a fraction of the vesicles in the sample.

To perform a more direct monitoring of the tube suppression and external tube generation, we externally added GM1 to the diluted vesicle solution while observing individual vesicles under microscope. The vesicle suspension was placed in a rectangular well-shaped sample chamber, which is open at the top and having a cover slip at the bottom. To a vesicle sample of 200 µl, we added from the top 1 µl of 0.1 mg/ml GM1 (~65 µM) dissolved in methanol/dichloromethane. A large fraction of the vesicles was observed to be damaged by the organic solvent. However, we could observe some of the vesicles over time to directly monitor the changes after the addition of GM1. Figure S2 summarizes the results. After preparation and tenfold dilution, the vesicle exhibits a large number of internal tubes, Fig. S2A. The vesicle thereafter was continuously monitored to observe the morphological changes after addition of the GM1 solution outside very slowly. Figure S2B-D shows the time lapsed images at 2 minutes intervals. A gradual disappearance of the tubes could be seen with time after increasing the concentration of GM1 in the exterior medium. After a longer time, even the appearance of large external nanotubes could be observed, see Fig. S2E. The observation conclusively shows the dependence of GM1 distribution between the membrane leaflets proportionately related to the concentration of free GM1 in the surrounding medium.

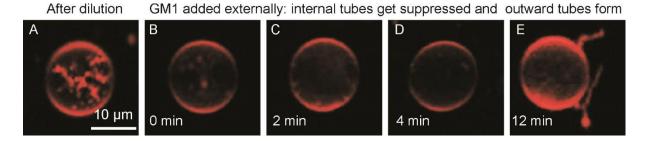


Fig. S2. Observations over a single vesicle with large number of internal tubes when subjected to addition of GM1 to the exterior medium. (A) Before adding GM1. (B-D) Images taken at 2-minute intervals showing the gradual disappearance of the tubes. (E) Around 12 min after the addition of GM1, the generation of large external tubes in the vesicle is observed.

S4. Electroporation of vesicles to measure the molar fractions of GM1 in the two membrane leaflets

For estimating the molar fractions of GM1 in membrane leaflets, first Alexa Fluor conjugated cholera subunit B (CTB-Alexa) was added to the vesicle solution at a concentration of 50 nM. Since the vesicles were intact, each CTB binds to five GM1 molecules present at the outer leaflet of vesicle membrane. After 10 min incubation, the vesicles were imaged under a confocal microscope (SP5 DMI 6000, Leica Microsystems Heidelberg GmbH, Germany) equipped with a 60 × HCX Plan APO objective (NA 0.75). Argon ion laser source at 495 nm was used to excite CTB-Alexa fluorescence. The bleaching of fluorescence over time was also monitored by time lapsed images of GUVs at intervals of 2 mins and no significant change could be seen for a total observation time of 30 min.

For pulse application, we used a modified electrofusion chamber (Eppendorf, Hamburg, Germany), which consists of a Teflon frame, a coverslip fixed at the bottom and a pair of parallel cylindrical electrodes with a radius of 92 μm and a separation of 0.5 mm fixed just above the bottom coverslip. Electric pulses of 50 ms duration and amplitudes ranging from 7 to 10 kV/m were applied directly under the microscope with a pulse generator (βtech, France). It has been previously reported that the critical poration potential depends on the initial membrane tension (3). Thus, the electroporation threshold can be different for each particular vesicle chosen depending on the initial tension. The pulse induces micron-sized pores in the vesicles and allows for inter-leaflet exchange of material as well as for CTB to access and bind to GM1 molecules in the inner leaflet of the vesicle membrane. After formation of large pores on the vesicles, a waiting period of ~10 minutes was allowed for CTB to bind to GM1 present in the inner membrane leaflet of the vesicles (see below and Fig. S3B).

The resulting increase in fluorescence can be used to assess the distribution of GM1 on both leaflets. We measured intensity line profiles across the membrane and along a circular path following the membrane contour as shown in Fig. S3A. While analyzing the porated vesicles, we left out the regions of the membrane with large number of outwardly hanging material as in the right panel of Fig. S3A. The time dependence of the fluorescence at the membrane is shown in Fig. S3B. It saturates already a couple of seconds after applying the electric pulse and stays constant during the pore lifetime suggesting that no unbinding of GM1 occurs.

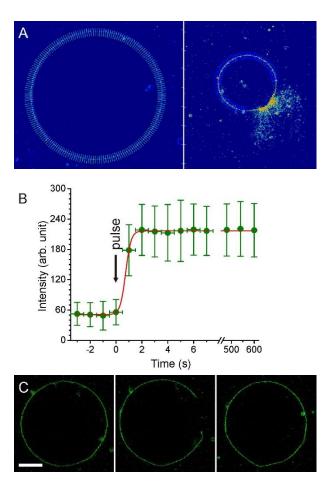


Fig. S3. Vesicle electroporation. (A) Image analysis to assess the GM1 distribution across leaflets. Two images (corresponding to those in Fig. 2A and 2C in the main text) and the lines along which the intensity line profiles following the membrane contours were acquired. The resulting intensity averages are displayed in Fig. 2D in the main text. (B) Time dependence of the membrane intensity before and during poration. The binding of CTB-Alexa to the membrane is saturated already in the first couple of seconds after opening the pore in the vesicle and stays constant until it closes (~10 min later). (C) Electroporation of a GUV with symmetric membrane. The vesicle exhibits no internal tubes which is an indication for spontaneous curvature close to zero. The confocal cross sections show the vesicle before (left), during (middle) and after (right) electroporation. Intensity profiles across the membrane (analyzed as explained in the main text) yield $I_{after}/I_{before} = 1.8$ for this vesicle. Scale bar, 25 μm.

As a control experiment, to confirm that the asymmetry is correctly represented by the ratio of membrane intensities before and after poration, I_{after}/I_{before} , we examined symmetric vesicles (presenting no tubes). One example (4 mol% GM1) is illustrated in Fig. S3C. On the average, we find $I_{after}/I_{before} = 1.9 \pm 0.4$ (the error represents standard deviation from measurements on 6 vesicles from different batches). The proximity of the value of the intensity ratio to 2 confirms the validity of the approach.

The vesicle response to electric pulses was observed also under phase contrast at high acquisition speed (30 000 frames per second), Fig. S4.

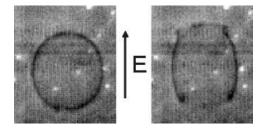


Fig. S4. A GUV (8 μm in diameter) exposed to a DC pulse (of field strength 1.5 kV/cm and duration 0.5 ms; the field direction is indicated with an arrow) exhibits large pores facing the electrodes as observed under phase contrast microscopy. At the pore rims, the membrane curls outward consistent with the negative spontaneous curvature resulting from the asymmetric GM1 distribution. The vesicles were prepared with 10 mol% GM1. The images before (left, 0 s) and at the end of the pulse (right, 0.5 ms) were acquired under phase contrast microscopy.

S5. Estimate for the GM1 concentrations on the inner and outer leaflets

After preparation, the vesicles are diluted tenfold unless otherwise specified (note that the degree of asymmetry depends both on the dilution as well as on the overall lipid concentration). After the dilution step, ϕ_{in} and ϕ_{out} are the molar fractions of GM1 in the inner and outer leaflets, respectively. With c_{in} and c_{out} we denote the molar concentrations of free GM1 inside and outside the vesicles, respectively. The partitioning equilibrium between bound and free GM1 is established on both sides of the membrane, therefore $\frac{\phi_{in}}{c_{in}}$ =

 $\frac{\phi_{out}}{c_{out}}$. From the measurements on the change of CTB fluorescence intensity, we know that

$$\frac{\phi_{in}}{\phi_{out}} = \bar{I} \equiv \frac{I_{after}}{I_{before}} - 1$$
, leading to

$$c_{in} = \bar{I}c_{out} \tag{S1}$$

The dilution is done by mixing a small aliquot v (100 μ l) from the prepared vesicle suspension with fresh (GM1-free) buffer to reach a total volume of V_t (1 ml). The volume of the electroformation chamber is V_{ch} (1.76 ml), of which the vesicles take a total volume of V_{ves} . The mass balance for GM1 in the diluted suspension gives

$$x\frac{n_{lip}}{2}(\phi_{in} + \phi_{out}) + xV_{ves}c_{in} + (V_t - xV_{ves})c_{out} = xn_{lip}\phi \qquad , \tag{S2}$$

where $x = v/V_{ch}$, n_{lip} is the lipid molar equivalent used for the preparation of the GUVs $(n_{lip} = 6.38 \times 10^{-8} \text{mole})$ and ϕ is the mole fraction of GM1 (2 mol% or 4 mol%) used for the vesicle preparation. The first term in Eq. S2 represent the moles of GM1 bound to the membrane (inner and outer leaflets), while the second and third terms reflect the amount of free GM1 inside and outside the vesicles, respectively. Above, we have assumed that no lipid loss during the vesicle electroformation occurs.

Before the dilution step, GM1 is symmetrically distributed across the membrane, $\phi_{in}^0 \equiv \phi_{out}^0$ and $c_{in}^0 \equiv c_{out}^0$. Evidence for this symmetry is that no tubes are observed after the vesicle preparation, and even after 24 hours of equilibration. Since the membrane is impermeable to GM1, the surface and bulk concentrations of GM1 inside the vesicles remain unchanged after dilution and thus $\phi_{in} = \phi_{in}^0$ and $c_{in} = c_{in}^0$. This also implies that $c_{out}^0 = c_{in}$ and $\phi_{out}^0 = \phi_{in}$. Then, mass conservation for GM1 (before and after the dilution) in the external solution and leaflet implies

$$x \frac{n_{lip}}{2} \phi_{out} + (V_t - xV_{ves})c_{out} = x \frac{n_{lip}}{2} \phi_{in} + x(V_{ch} - V_{ves})c_{in}$$
 (S3)

where the right-hand side represents the initial amount of GM1 in the outer leaflet and in the medium corrected by the dilution factor. Assuming that the total amount of lipids is involved in forming vesicles of radius ~10 μ m and taking for the molecular area of POPC ~68 Å² (4), and $n_{POPC} \cong n_{lip} = 6.38 \times 10^{-8}$ mole, for the volume enclosed in the vesicles before the dilution we obtain $V_{ves} = 0.0436$ ml. This volume represents a negligible correction, $V_{ves} \ll V_{ch} \ll V_t/x$, and will be ignored. Inserting Eq. S1 in Eq. S2 gives

$$c_{out} = n_{lip} \frac{\phi - (\phi_{in} + \phi_{out})/2}{V_t / x + V_{ves} \bar{I}}$$
 (S4)

Introducing this expression in Eq. S3 and after some algebra, we obtain

$$\phi_{out} \cong \frac{\phi}{\bar{I}} \left[1 + \frac{xV_{ves}}{V_{ch}} (1 - \bar{I}) \right]$$
 (S5)

The results for the two vesicle compositions used are shown in Table 1 in the main text.

S6. Optical tweezers and force measurement

The optical tweezers (5, 6) was built around a motorized inverted microscope (Axiovert 200M, Zeiss) and comprises of a single beam optical tweezers formed by focusing a

1064 nm, cw laser beam from a Nd:YAG laser (Spectra Physics, USA) through a 100×, NA 1.25 objective lens (Acroplan, Zeiss). Typical laser powers used were ~0.8 W at the sample. The microscope was equipped with a motorized stage (LStep13, Märzhäuser) that can be used to position and translate the sample chamber with a resolution of 50 nm and speed of 1-500 μm/s respectively. All measurements were performed at ~23°C. Images were captured by an EMCCD camera (ImagEM, Hamamatsu Corp) at 30 frames per second. ImageJ was used for size and coordinate analysis of vesicles using edge detection technique. The optical tweezers was used to trap latex microspheres (Polyscience Inc.) of $2 \pm 0.045 \,\mu m$ diameter attached to the GUV membrane and therefore manipulating these to pull tubes. The tube pulling forces were estimated by monitoring the position shift of the trapped bead from the trap center, $f = -K_{trap}(x - x_0)$, where $x - x_0$ is the position shift of the trapped bead from the trap center (x_0) when a tube is pulled and K_{trap} is the stiffness of the trap. The calibration parameter K_{trap} was determined by drag-force method in which the motorized stage was used to drag a trapped bead through the chamber at several fixed velocities. During the stage movement, hydrodynamic forces act on the bead as $f_{drag} = 6\pi \eta R_{bead} U$, where η is the viscosity of the solution, R_{bead} is the radius of the bead and U is the velocity at which it is moved. The bead was imaged using the CCD camera and its position was determined using centroid tracking algorithm (7) written in MATLAB (Mathworks Inc). The precision of position sensing using the centroid tracking technique could be estimated to be ~4 nm and ~6 nm along x and y directions, respectively. All measurements were performed at a height of ~ 20 µm from the bottom glass boundary of the sample chamber. The stiffness of the tweezers was found to be ~88 pN/µm for typical laser power above the objective (at sample height) of 0.8 W. Once the stiffness was known, subsequent imaging and determining bead displacement allowed us to estimate the net tube pulling force acting on the bead by off-line analysis with a temporal resolution of ~ 33 ms.

S7. Micropipette manipulation of GUVs

For each experiment, a 5 mm wide, 15 mm long and 2 mm deep chamber was built by fixing one ~130 µm thick glass coverslip and 1 mm thick glass slide against each other separated by spacers. To prevent adhesion of the vesicles to the glass surfaces, the chamber and the micropipette were passivated by coating with 1 mg/ml BSA then rinsed with buffer containing 1 mM HEPES (pH 7.4). The chamber was mounted on the microscope and the vesicle solution was introduced. A single micropipette was inserted into the sample chamber

with the use of a three-dimensional micromanipulator system (Narishige Corp, Japan) clamped on the microscope. Following insertion, zero pressure across the pipette tip was attained and calibrated by watching the flow of small particles within the tip. Aspiration pressure was controlled through adjustments in the height of an attached mobile water reservoir mounted on a linear translational stage (M-531.PD; Physik Instrumente, Germany). This allowed for varying the membrane tension of the GUV from 1×10^{-6} to 3×10^{-4} N/m.

In order to obtain a projection length greater than the pipette radius at low aspiration pressures, vesicles with a low initial membrane tension were selected. For pulling inward tubes, first, a latex bead was trapped using the optical tweezers. Then, the aspirated vesicle was brought into contact with the bead and manipulated across the vesicle surface through the region opposite of the pipette. After that, the separation between the bead and vesicle membrane is increased to extend the tube to a suitable length (typically around 10 µm); this length was kept constant during the whole experiment. Membrane tension was then increased by steps. For each tension, the position of the bead relative to the trap center was recorded by video microscopy. For studying the spontaneous curvature of GM1, the waiting time between a pressure change and image acquisition was about 2 min in order to reach the equilibrium composition in the tube by lipid diffusion. This time scale is consistent with the time required for a lipid to explore a $\sim 10 \mu m$ long membrane tube with a typical diffusion constant of 5 μm²/s (8). Before each set of experiments on a new vesicle, the zero reference pressure in the pipette was set by detecting the absence of movement of a bead in the pipette. For the experiments shown in Fig. 3E,F, the suction pressure of the pipette was changed from ~ 19.6 Pa to ~ 68.7 Pa, corresponding to changing heights of the water reservoir from 2 mm to 7 mm. The pressure change was typically done in five equal steps. The corresponding membrane tension could be estimated from Eq. 4 in the main text. All experiments were performed at room temperature, 23±1°C.

S8. Extruding inward and outward tubes from GM1-doped vesicles

For pulling an in-tube, a GUV was first held by the micropipette under very low aspiration pressure (~ 5 Pa) and thereafter taken into contact of a trapped latex bead. After allowing few minutes of contact between the latex bead and the membrane lipid, the GUV was slowly pressed to the trapped bead to cause it to bend the membrane inward and move inside of the vesicle via gradual wetting by the fluid membrane. The wetting of the trapped bead in the fluid membrane causes a natural adherence to occur between the lipid and the bead (9), and

thereafter, when increasing the separation between the bead and the vesicle membrane by translating the GUV further, an in-tube could be formed. The fluorescence from TR-DHPE could be used to image the membrane nanotube. A long sequence (one thousand frames) of bright-field images were recorded and therefore analyzed for measuring the position of the trapped bead to estimate the tube pulling force. The vesicle membrane tension could be subsequently set at higher values by applying higher suction pressure of the pipette and similar measurements were carried out to estimate the pulling forces. Afterwards, the vesicle membrane tension was reduced to a small value and the aspirated vesicle was moved in the opposite direction to manipulate the trapped bead towards the exterior of the vesicle. Subsequent increase in the separation between the vesicle and the bead cause the formation of an outward tube, on which similar measurements were carried out. During manipulation of the bead through the vesicle membrane, the mechanical tension over the membrane had to be reduced to a small value (typically ~ 0.01 mN/m) otherwise we observed that the bead can get dislodged out of the optical trap due to elastic forces of the membrane. The pulling force and the vesicle aspiration system were allowed to briefly equilibrate before initiating acquisition of images.

Figure S5 displays the difference between the force for pulling outward and inward tubes $f_{out} - f_{in} = -8\pi\kappa m$ on the same vesicle. Within the error, the force difference does not depend on the vesicle tension and can be used to deduce the membrane spontaneous curvature provided the bending rigidity is known or vice versa.

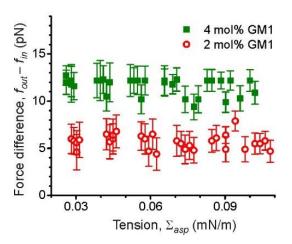


Fig. S5. Force difference $f_{out} - f_{in}$ for pulling outward and inward tubes on the same vesicle as a function of the membrane tension. The collected data is from 5 different vesicles for each membrane composition.

S9. Measuring the threshold tension at which tubes reform

In addition to tube pulling experiments performed to evaluate the threshold tension below which tubes spontaneously reform (black data in Fig. S6 assessed from $\Sigma^0_{asp} = 2\kappa m^2$), we measured this tension using micropipette aspiration and vesicle electrodeformation (2, 10), red data in Fig. S6. The latter methods were applied to explore membranes at higher concentration of GM1 and were thus performed at 40°C to avoid phase separation (2). All methods give consistent trend.

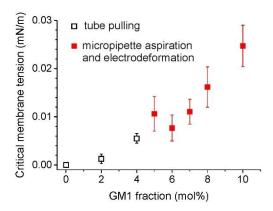


Fig. S6. Threshold membrane tension below which internal tubes reform into the vesicle body. For lower GM1 fractions (black squares), the data was collected from tube pulling experiments where the plotted critical tension corresponds to Σ_{asp}^0 as assessed from the intercept of the data in Fig. 3F in the main text with the horizontal axis, see Eq. 8 in the main text. For higher GM1 fractions (red squares), the data was collected from micropipette aspiration and vesicle electrodeformation.

S10. Coarse-grained molecular dynamics simulations

We used the fast, flexible and free GROMACS (11-18) engine version 5.1.1 to run MARTINI (19) coarse-grained molecular dynamics simulations with the MARTINI-straight parameters (20). The GM1-containing POPC bilayers at full hydration, with sodium ions to obtain zero net charge, were simulated at 303 K and 1 bar. We first used the GM1 parameterization developed by López et al. (21), but observed strong clustering behavior of GM1 in this model, see Fig. S7A and Ref. (22). We thus built a new GM1 model by combining the bonded parameters of López et al. (21) with the non-bonded parameters of Gu et al. (22). This new model was free of the clustering artifact (see Fig. S7A), while maintaining the GM1 shape of the López model (Fig. S7B). Like the López model (Fig. S8B), it reproduced quantitatively our experimental data (Fig. 4 in the main text), while the

Gu model (22) did not. The lateral stress profiles of the bilayers were calculated with GROMACS-LS (23); only the Goetz-Lipowsky decomposition (24) could be used, as the Central Force Decomposition (25) diverges with the dihedral potentials present in the MARTINI GM1. The simulation box dimensions (x/y/z) were roughly 8 nm/8 nm/10 nm. The simulation lengths for the López model were 400 μ s (except for the $\phi_{in} \mid \phi_{out} = 1 \mid 1$ system, 100 μ s) with sampling rate of 500 ps. For our new model, the simulation length was 100 μ s (except for the $\phi_{in} \mid \phi_{out} = 1 \mid 1$ system where it was 20 μ s) with sampling rate of 100 ps. The number of independent samples for the standard error of the mean was determined by the blocking method (26). Due to the long-lived structural correlations caused by the GM1 clustering, in some of the simulations with the López model $\{\phi_{in} \mid \phi_{out} = 1 \mid 0; 2 \mid 0; 1 \mid 1; 9 \mid 1\}$ the blocking method failed to find a plateau spanning two orders of magnitude in time; for these systems the error was estimated by visually assessing the cumulative average.

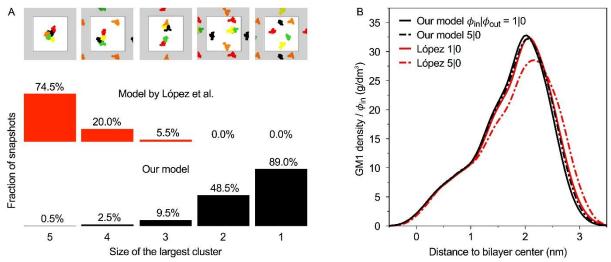


Fig S7. The two GM1 models examined here have drastically different GM1 clustering behavior. (A) Cluster size distributions observed in simulations with $\phi_{in} = 5$; $\phi_{out} = 0$. Snapshots categorized by the size of largest GM1 cluster: the top row shows an example for each category (each GM1 head group differently colored; view along the membrane normal; periodic images of the simulation box are shaded in gray). Fraction of snapshots of specific cluster size (cluster size 1 corresponds to non-clustered GM1) according to López et al. (21) and the model developed here. (B) The density profiles over the inner leaflet, normalized by the number of GM1s (ϕ_{in}), show that when alone ($\phi_{in} = 1$) the GM1 shapes in the two models were practically indistinguishable, and that clustering (seen for López $\phi_{in} = 5$, c.f. panel A) extended the GM1s slightly.

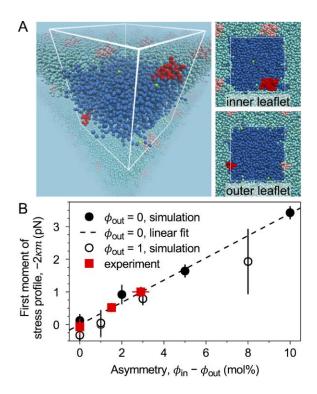


Fig S8. Simulation results for the GM1 model by López et al. (21) and comparison with experimental data from this work. (A) A simulation snapshot of the inner bilayer leaflet (upper monolayer within the white wireframe) and the outer leaflet (lower monolayer) for GM1 molar fractions $\phi_{in} = 4$ mol% and $\phi_{out} = 1$ mol% using the MARTINI coarse-grained molecular dynamics simulation model with GM1 parameters developed by López et al. (21). Leaflet-wise mole fractions directly indicate the numbers of lipids: $\phi_{in} = 4$ corresponds to 4 GM1 and 96 POPC molecules in the inner leaflet. The white wireframe with the strongly colored species (GM1 red, POPC blue, sodium green, water not shown) shows the simulation box, and the lightly colored molecules indicate its periodic images. (B) Comparison of simulation results to experiments. The first moment of the lateral stress profile $(-2\kappa m)$ is plotted as a function of the bilayer asymmetry $\phi_{in} - \phi_{out}$ for bilayers when the outer leaflet is pure POPC ($\phi_{out} = 0$, solid circles), and when it contains one GM1 ($\phi_{out} = 1$, open circles). The dashed line represents the linear fit $-2\kappa m = 0.34(\phi_{in} - \phi_{out})$ to the data for $\phi_{out} = 0$. As for our model (see Fig. 4 in the main text), the dependence is quantitatively consistent with the experimental results (red squares) obtained from the pulling force for vanishing tension, see Eq. 9 in the main text.

References

- 1. Dimova R, et al. (2006) A practical guide to giant vesicles. Probing the membrane nanoregime via optical microscopy. J. Phys.: Condens. Matter 18(28):S1151-S1176.
- 2. Fricke N & Dimova R (2016) GM1 Softens POPC Membranes and Induces the Formation of Micron-Sized Domains. *Biophys. J.* 111(9):1935-1945.
- 3. Riske KA & Dimova R (2005) Electro-deformation and poration of giant vesicles viewed with high temporal resolution. *Biophys. J.* 88(2):1143-1155.

- 4. Kucerka N, Tristram-Nagle S, & Nagle JF (2005) Structure of fully hydrated fluid phase lipid bilayers with monounsaturated chains. *J. Membr. Biol.* 208(3):193-202.
- 5. Kraikivski P, Pouligny B, & Dimova R (2006) Implementing both short- and long-working-distance optical trappings into a commercial microscope. *Rev. Sci. Instrum.* 77(11):113703.
- 6. Dasgupta R & Dimova R (2014) Inward and outward membrane tubes pulled from giant vesicles. *J Phys D Appl Phys* 47(28):282001.
- 7. Dasgupta R, Verma RS, & Gupta PK (2012) Microfluidic sorting with blinking optical traps. *Opt. Lett.* 37(10):1739-1741.
- 8. Lipowsky R & Sackmann E (1995) *Structure and dynamics of membranes* (Elsevier Science, Amsterdam; New York) pp v. <1A-1B, >.
- 9. Dietrich C, Angelova MI, & Pouligny B (1997) Adhesion of latex spheres to giant phospholipid vesicles: statics and dynamics. *J. Phys. II* 7(11):1651–1682.
- 10. Gracià RS, Bezlyepkina N, Knorr RL, Lipowsky R, & Dimova R (2010) Effect of cholesterol on the rigidity of saturated and unsaturated membranes: fluctuation and electrodeformation analysis of giant vesicles. *Soft Matter* 6(7):1472-1482.
- 11. Bekker H, et al. (1993) Gromacs a Parallel Computer for Molecular-Dynamics Simulations. *Physics Computing '92*:252-256.
- 12. Berendsen HJC, Vanderspoel D, & Vandrunen R (1995) Gromacs a Message-Passing Parallel Molecular-Dynamics Implementation. *Comput. Phys. Commun.* 91(1-3):43-56.
- 13. Lindahl E, Hess B, & van der Spoel D (2001) GROMACS 3.0: a package for molecular simulation and trajectory analysis. *J. Mol. Model.* 7(8):306-317.
- 14. Van der Spoel D, *et al.* (2005) GROMACS: Fast, flexible, and free. *J. Comput. Chem.* 26(16):1701-1718.
- 15. Hess B, Kutzner C, van der Spoel D, & Lindahl E (2008) GROMACS 4: Algorithms for highly efficient, load-balanced, and scalable molecular simulation. *Journal of Chemical Theory and Computation* 4(3):435-447.
- 16. Pronk S, et al. (2013) GROMACS 4.5: a high-throughput and highly parallel open source molecular simulation toolkit. *Bioinformatics* 29(7):845-854.
- 17. Pall S, Abraham MJ, Kutzner C, Hess B, & Lindahl E (2015) Tackling Exascale Software Challenges in Molecular Dynamics Simulations with GROMACS. *Lect Notes Comput Sc* 8759:3-27.
- 18. Abraham MJ, et al. (2015) GROMACS: High performance molecular simulations through multi-level parallelism from laptops to supercomputers. *SoftwareX* 1–2:19-25.
- 19. Marrink SJ, Risselada HJ, Yefimov S, Tieleman DP, & de Vries AH (2007) The MARTINI force field: Coarse grained model for biomolecular simulations. *J. Phys. Chem. B* 111(27):7812-7824.
- 20. de Jong DH, Baoukina S, Ingolfsson HI, & Marrink SJ (2016) Martini straight: Boosting performance using a shorter cutoff and GPUs. *Comput. Phys. Commun.* 199:1-7.
- 21. López CA, Sovova Z, van Eerden FJ, de Vries AH, & Marrink SJ (2013) Martini Force Field Parameters for Glycolipids. *Journal of Chemical Theory and Computation* 9(3):1694-1708.
- 22. Gu R-X, Ingólfsson HI, de Vries AH, Marrink SJ, & Tieleman DP (2017) Ganglioside-Lipid and Ganglioside-Protein Interactions Revealed by Coarse-Grained and Atomistic Molecular Dynamics Simulations. *J. Phys. Chem. B* 121(15):3262-3275.
- 23. Vanegas JM, Torres-Sanchez A, & Arroyo M (2014) Importance of Force Decomposition for Local Stress Calculations in Biomembrane Molecular Simulations. *Journal of Chemical Theory and Computation* 10(2):691-702.
- 24. Goetz R & Lipowsky R (1998) Computer simulations of bilayer membranes: Self-assembly and interfacial tension. *J. Chem. Phys.* 108(17):7397-7409.
- 25. Admal NC & Tadmor EB (2010) A Unified Interpretation of Stress in Molecular Systems. *J Elasticity* 100(1-2):63-143.

26.	Flyvbjerg H & Petersen HG (1989) Error-Estimates on Averages of Correlated Data. <i>J. Chem. Phys.</i> 91(1):461-466.